

Corpus Callosum Atrophy Correlates with Gray Matter Atrophy in Patients with Multiple Sclerosis

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ABSTRACT

OBJECTIVE

Atrophy of the corpus callosum is a recognized characteristic of multiple sclerosis (MS). We describe a new reliable method for measuring corpus callosum atrophy and correlate this with global cerebral atrophy measures.

METHODS

Whole brain 3T MRI was performed in 38 relapsing-remitting MS subjects and 21 healthy controls (HC). Brain global gray and white matter volumes were segmented with SPM8. The contour of the corpus callosum was outlined on the midline of 3-D T1-weighted images by a semiautomated edge-detection technique to determine the corpus callosum area (CCA). Normalized CCA was correlated with other brain atrophy measures in MS subjects.

RESULTS

CCA was disproportionately lower in MS subjects vs. HC (20.1% mean decrease; $P < .001$), with a large effect size ($d = .62$) when compared with global atrophy measures. In MS subjects, CCA correlated with brain parenchymal fraction ($r = .55$; $P < .001$) and gray matter fraction ($r = .45$; $P = .005$) but not white matter fraction ($r = .18$; $P = .29$). An inverse correlation with FLAIR hyperintense lesion volume ($r = -.40$; $P = .01$) was detected for CCA.

CONCLUSION

Measurement of atrophy of the corpus callosum can have sensitivity as a useful imaging biomarker in patients with MS, even in patients with low disability levels. Both gray and white matter involvement in MS contribute to corpus callosum atrophy.

Keywords: Multiple sclerosis, corpus callosum, atrophy.

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Introduction

Cerebral atrophy is a clinically relevant manifestation of multiple sclerosis (MS) pathology.^{1,2} Atrophy can occur early in the disease course and is considered a substrate for clinical disability and cognitive dysfunction.³ Atrophy occurs differentially in the gray matter (GM) and white matter (WM) in MS and may contribute to various aspects of MS-related cognitive dysfunction.⁴

Examples of GM structures most vulnerable to early atrophy in MS include the thalamus and the hippocampus.^{5,6} The corpus callosum, the compact WM bundle connecting the two hemispheres, represents a WM region of distinct interest because of the predilection for MS pathology.^{7,8} The exact mechanism of

corpus callosal atrophy is not clearly understood and may include the direct result of focal lesions, Wallerian degeneration from MS pathology in adjacent WM areas, or a secondary effect of neurodegenerative processes in GM. Prior studies have associated corpus callosum atrophy with the level of disability in MS.^{9,10} Furthermore, the corpus callosum is implicated in cognitive dysfunction in MS and its involvement may disrupt inter-hemispheric connectivity.¹¹⁻¹⁶ The relationship between corpus callosum damage and cognitive dysfunction can be shown even in benign MS.¹⁷

In this study, we sought to describe a new method to assess callosal atrophy from 3T MRI and characterize its relationship to global cerebral atrophy.

Table 1. Demographic, Clinical, and MRI Data

	Healthy Controls	RRMS
Subjects	21	38
Sex ratio (males/females)	5/16	13/25 ($P = .41$)
Age (years), mean \pm SD (range)	44 \pm 6.8 (30-53)	40 \pm 7.8 (21-53) ($P = .026$)
Disease duration (years), mean \pm SD (range)	N/A	8.0 \pm 5.9 (1-28)
EDSS, median (range)	N/A	1.0 (0-3.5)
25-foot timed walk (seconds), mean \pm SD (range)	N/A	4.1 \pm .7 (2.9-6.5)
FLAIR lesion volume (mm^3), mean \pm SD (range)	N/A	8848 \pm 11453 (80-52411)

N/A = not applicable; EDSS = expanded disability status score; FLAIR = fluid attenuated inversion recovery; RRMS = relapsing-remitting multiple sclerosis.

Methods

Standard Protocol Approvals, Registrations, and Patient Consents

Informed consent was obtained from all subjects under the Partners Institutional Review Board.

Subjects

General demographic and clinical data were obtained from 38 relapsing-remitting (RR) MS subjects and 21 age-matched healthy controls (HC; Table 1). All MS subjects met McDonald diagnostic criteria.¹⁸ Other inclusion criteria included no relapse or corticosteroid use within 4 weeks before study entry (to avoid transient confounding effects on MRI) and absence of another major medical disorder. At the time of enrollment, MS subjects were on treatment with glatirimer acetate ($n = 16$), interferon beta ($n = 16$) or no disease-modifying therapy ($n = 6$). All subjects underwent a 25 foot timed walk and the Expanded Disability Status Scale (EDSS) examination by MS specialist neurologists. HC for this study were recruited as described previously.¹⁹

Image Acquisition

All subjects underwent whole brain MR imaging at 3T (Signa; GE Healthcare, Milwaukee, WI, USA), using the same scanning protocol. Imaging was performed using a multichannel head-only phased array coil. Brain imaging sequences included the following:

1. Axial FLAIR: TR = 9000 ms, TE = 151 ms, TI = 2250 ms, section thickness = 2 mm (70 sections, no gap), matrix size = 256×256 , pixel size = $.976 \times .976$ mm, number of signal averages = 1, acquisition time ~ 9 minutes.
2. Coronal 3-D modified driven equilibrium Fourier transform (MDEFT)²⁰: TR = 7.9 ms, TE = 3.14 ms, flip angle = 15° , section thickness = 1.6 mm (124 sections, no gap), matrix size = 256×256 , pixel size = $.938 \times .938$ mm, number of signal averages = 1, acquisition time ~ 7.5 minutes.

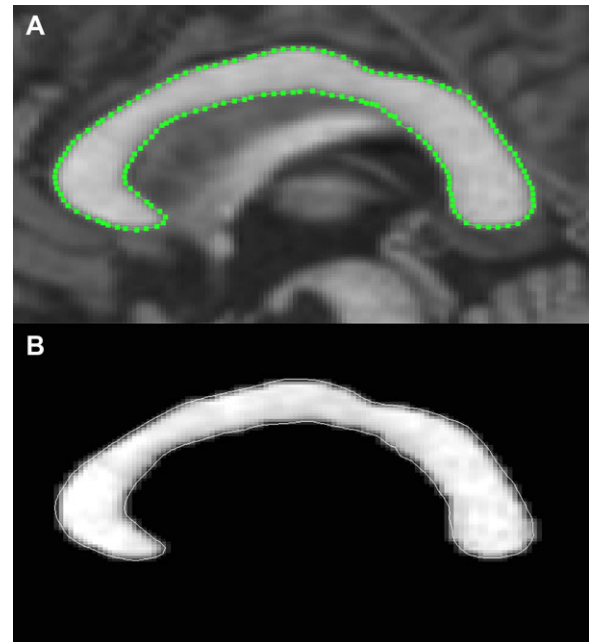


Fig 1. Corpus callosum area determination from 3-D T1-weighted MDEFT images obtained with 3T MRI. (A) Using a semiautomated edge detection method, an ROI is created for the midline of the corpus callosum. (B) The corpus callosum is visualized as a masked view for cross sectional area determination.

All image analysis was performed in a blinded manner, without knowledge of group assignment or clinical information.

Corpus Callosum Area (CCA) Determination

An expert observer (ECK) blinded to clinical information performed CCA determination. The MDEFT images were re-sampled (1.6 mm slice thickness) in the sagittal anterior commissure (AC) to posterior commissure (PC) plane in a new, in-house developed method to accurately represent the midline of the corpus callosum using Jim software (v5.0, Xinapse Systems, Northants, United Kingdom). A midsagittal slice was selected in the AC-PC plane for further analysis. Intensity normalization was applied with a maximal intensity of 1.2 times the intensity of the splenium of the corpus callosum (a relatively high intensity region of the corpus callosum) on MDEFT images to help standardize edge detection of the corpus callosum. The contour of the corpus callosum was outlined by a semiautomated edge-detection technique to determine the CCA (Fig 1). The intra- and inter-rater observer (two observers—ECK and AA) variability was assessed by intraclass correlation coefficient (ICC) analysis in a subset of randomly chosen six MS patients.

Global Cerebral Image Segmentation and Lesion Determination

MDEFT scans were deskulled using a semi-automated tool in the Jim software package. The intracranial volume (ICV) was used to normalize all atrophy-related volume measurements.

Manually skull stripped MDEFT images were first brought into approximate alignment with the ICBM template, then bias-field corrected, spatially normalized and automatically

Table 2. Differences in Volumetric Measures between Controls and RRMS

	Healthy Controls (Mean \pm SD)	RRMS (Mean \pm SD)	% Decrease (Controls vs. RRMS)	Effect Size Cohen's <i>d</i>	<i>P</i> Value
CCA	5.36 \pm .64	4.29 \pm .73	20.1%	.62	<.001
BPF	.846 \pm .015	.826 \pm .032	2.3%	.39	.004
GMF	.527 \pm .022	.517 \pm .016	2.0%	.20	.036
WMF	.318 \pm .020	.310 \pm .022	2.8%	.22	.222

CCA = normalized corpus callosum area; BPF = brain parenchymal fraction; GMF = gray matter fraction; WMF = white matter fraction; RRMS = relapsing-remitting multiple sclerosis.

segmented into GM, WM, and CSF probability maps using the unified segmentation model implemented in the segmentation routine of SPM8²¹ running in Matlab (version 2009a, The MathWorks, Inc., Natick, MA, USA). Within manual outlines of the intracranial cavities, mutually exclusive masks for each tissue were derived from SPM8 tissue probability maps as described previously.²² Estimates of WM volume (WMV), GM volume (GMV), CSF volume, and brain parenchymal volume (BPV = WMV + GMV) were automatically derived from SPM8 generated segmentations after corrections for T1-hypointense lesion-related misclassifications and deep GM underestimation as previously described.²³ These values were used to compute normalized compartment volumes: WM fraction (WMF = WMV/ICV), GM fraction (GMF = GMV/ICV), and brain parenchymal fraction (BPF = [WMV + GMV]/ICV).

Whole brain FLAIR lesion volume (FLV) was obtained by a semiautomated edge-finding method based on local thresholding as previously described.²⁴

Statistical Analysis

CCA measurements were normalized by ICV to the 2/3 power. CCA and volumetric measures were compared between MS subjects and HC using multiple linear regression (with age and sex as covariates). Effect size was determined using Cohen's *d*, defined as the difference between the two means divided by the standard deviation of the data.²⁵ CCA was correlated with other brain atrophy measures in MS subjects using Pearson's correlation coefficient, with FLV using Spearman's correlation coefficient, and with EDSS using Kendall's tau-b. A *P* value of <.05 was considered significant. Statistical analyses utilized the Statistical Package for the Social Sciences (SPSS, v. 21, Chicago, IL, USA).

Results

Corpus Callosum Area

Intrarater reliability (ICC = .98) and inter-rater reliability (ICC = .96) were high and included all aspects of the new CCA method, starting with resampling. When determining differences between MS and controls, age was added to the model to control for any confounding effect. Group differences in imaging outcomes are shown in Table 2. CCA was lower in MS subjects versus HC (20.1% mean decrease; *P* < .001; Fig 2). The effect size for CCA (*d* = .62) was greater than any of the global atrophy measures (BPF, 2.3% decrease, *P* = .004, *d* = .39; GMF, 2.0% decrease, *P* = .036, *d* = .20; WMF, 2.8% decrease, *P* = .222, *d* = .22). Thus, the corpus callosum showed selec-

tive disproportionate atrophy vs. global cerebral measures in patients with RRMS.

MRI Correlates of Corpus Callosum Atrophy

CCA did not correlate with BPF, GMF, or WMF in control subjects (all *P* > .05, data not shown). Figure 3 shows simple scatterplots detailing the relationship between CCA and other MRI measures in MS subjects. CCA correlated with BPF (*r* = .55; *P* < .001) and GMF (*r* = .45; *P* = .005), but not WMF (*r* = .18; *P* = .29). An inverse correlation with FLV (*r* = -.40; *P* = .01) was detected for CCA, indicating a relationship between WM lesions and corpus callosum degeneration.

Clinical Correlates of Corpus Callosum Atrophy

There was a trend for correlation of CCA with EDSS score (tau = -.23; *P* = .06). Of the volumetric atrophy measures, only BPF correlated with EDSS (BPF, tau = -.33; *P* = .011; GMF, tau = -.20, *P* = .11; WMF, tau = .20; *P* = .11). CCA did not correlate with disease duration (*r* = .05; *P* = .43) or 25-foot timed walk (*r* = -.19; *P* = .23) in MS subjects. Only BPF correlated with 25-foot timed walk (*r* = .40; *P* = .014).

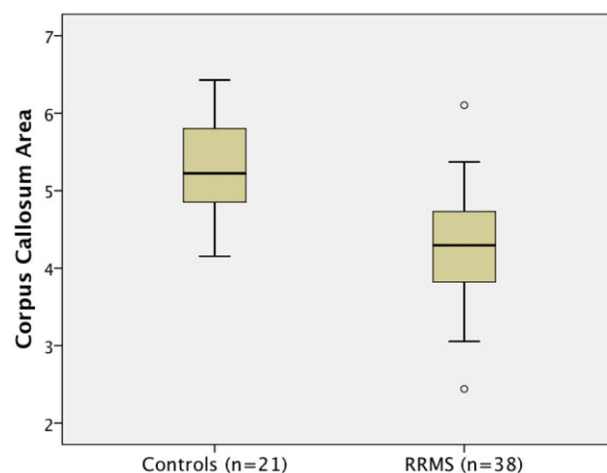


Fig 2. Box plot of corpus callosum area by subject group. Corpus callosum area was lower in MS subjects versus HC (20.1% mean decrease; *P* < .001). Boxes represent 25th-75th percentiles. Whiskers represent two standard deviations from the mean. Outliers are represented by circles.

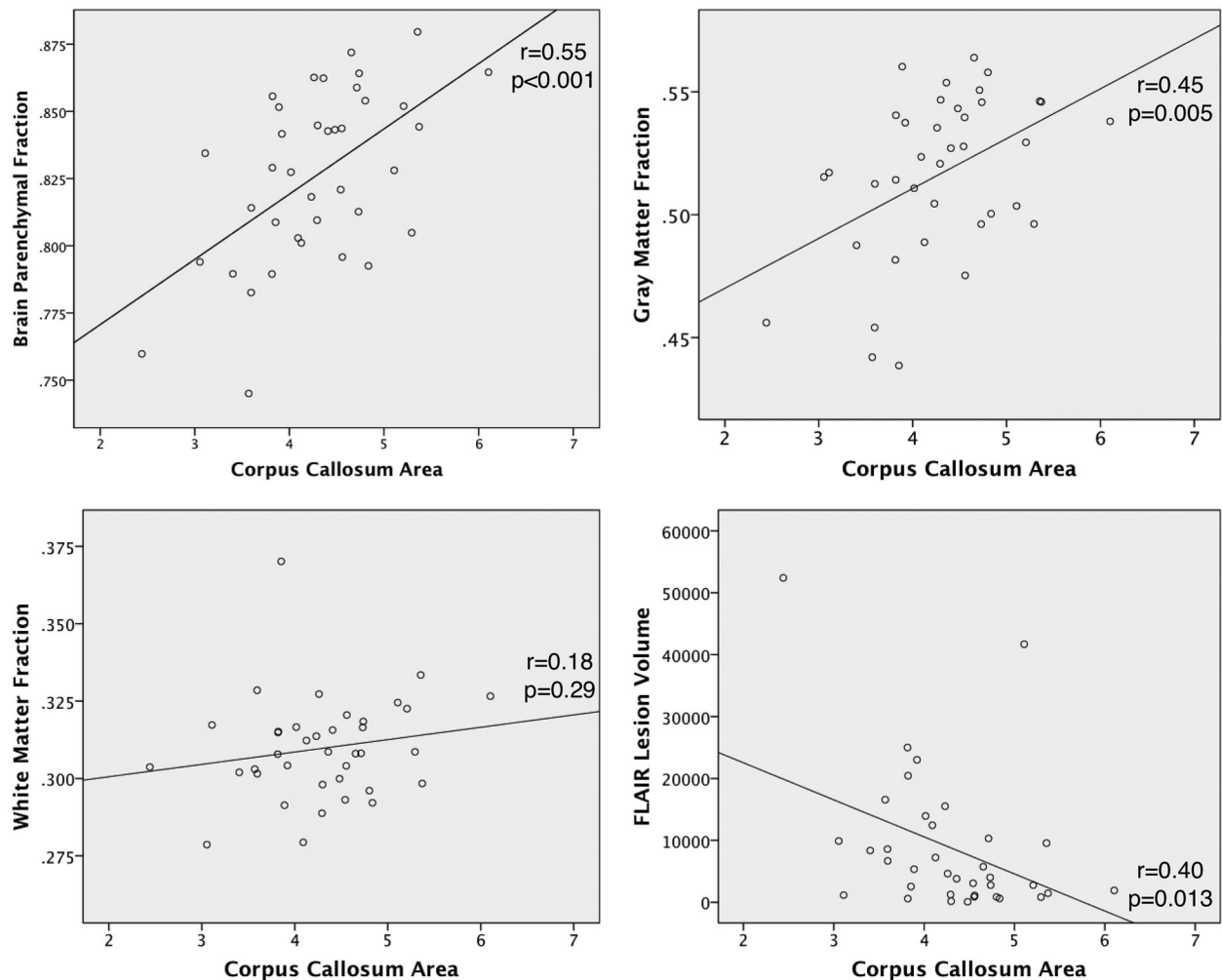


Fig 3. Correlation of corpus callosum area (CCA) with brain parenchymal fraction (BPF), gray matter fraction (GMF), and white matter fraction (WMF). A scatterplot of CCA versus BPF ($r = .55$; $P < .001$) and CCA versus GMF ($r = .45$; $P = .005$) show moderate significant correlations. A scatterplot of CCA versus WMF shows no correlation ($r = .18$; $P = .29$). FLV versus CCA demonstrate an inverse correlation ($r = .40$; $P = .013$).

Discussion

We describe an optimized method that reliably quantifies corpus callosum atrophy. We evaluated corpus callosum atrophy in relationship to common measures of whole brain and compartment-specific global cerebral atrophy in a group of HC and RRMS subjects. CCA was disproportionately low in MS and displayed a larger effect size than other measures of atrophy. Corpus callosum atrophy correlated with BPF, GMF, WM lesions, and trended toward correlation with EDSS.

In this study, we introduce a novel optimized approach to segmenting the corpus callosum. This was based on previous methods with the addition of image resampling and intensity normalization.¹⁰ There are several possible ways of quantifying atrophy of the corpus callosum. Volumetric measures of the corpus callosum suffer from inexact determinations of the lateral margins of the corpus callosum. Several corpus callosum parcellation schemes have been used previously, but here we relied

on cross sectional area of the entire corpus callosum.²⁶ Other methods have used 1-dimensional corpus callosum thickness to estimate corpus callosum atrophy in a simplified method that can be performed easily on clinical MRIs.^{16,27} Our new method is based on the notion that area measures in the midsagittal plane may reflect the total corpus callosum volume. With our technique, steps were taken, including resampling images, to analyze the exact midsagittal slice of corpus callosum to provide a reliable 2-dimensional quantitative outcome, CCA. We aimed to normalize CCA for head size using ICV, similar to methods used to normalize GMV and WMV to derive GMF and WMF. This method uses a resampled single sagittal slice, which offers the advantage of simplicity in measurement. Although only a single slice is used, the uniformity of the corpus callosum implies that a midsagittal slice should be representative. This led to a highly reliable estimation of corpus callosum volume, shown by high intra- and interclass correlation. Although we have not as yet tested the longitudinal

sensitivity of our methods, we hypothesize that this measure can be easily incorporated into therapeutic clinical trials and even clinical settings.

Even in a group of MS subjects with relatively low levels of disability, atrophy of the corpus callosum was significant, similar to other studies of early onset MS with mild disability.²⁸ In our study, corpus callosum atrophy was evident to a greater extent than other commonly derived global atrophy measures such as BPF, GMF, and WMF. When compared to HC, the effect size of CCA in MS was greater than any other atrophy outcome evaluated. A different study examining CIS patients, showed that a >1% change in CCA over 6 months predicted conversion to clinically definite MS (CDMS).²⁹ In the same study, GM atrophy was not a predictor of conversion to CDMS and was not different between CIS and CDMS groups. This provides some evidence that the corpus callosum may be a sensitive tool to monitor the destructive aspects of the disease even in patients with mild disability and who are early in their disease course.

A strength of this study includes the correlation of CCA with other imaging outcomes. Surprisingly, corpus callosum atrophy correlated with GMF but not WMF, even though the corpus callosum makes up a component of the WM. It is possible this could reflect a technical limitation of measurement of WM atrophy, confounded by transient inflammatory and fluid-related changes.³⁰ Corpus callosum atrophy significantly correlated with FLV, suggesting a component of this atrophy may be related to WM disease and Wallerian degeneration. In the HC group, there was no association between CCA and any other volumetric measure. This suggests that corpus callosum atrophy occurs in concert with reductions in GMF, although may not be directly related to it. This finding is supported by a study by Bendfeldt et al. who assessed the association between WM lesion distributions and GMV changes.³¹ They found that WM lesion changes in the corpus callosum and optic radiations were associated with cortical GMV reductions. Current understanding of cortical atrophy suggests that this process, perhaps related in part to cortical demyelination, may occur by a different mechanism than atrophy of the corpus callosum.³² Mechanistically, our study suggests that both GM and WM processes contribute to corpus callosum atrophy.

Disability level trended toward correlation with CCA, unlike a previous study¹⁶ using a different measure of corpus callosum atrophy; although the MS subjects we studied overall had a mild level of disability, limiting the range of disability levels studied. Even so, this adds to significance of corpus callosum changes demonstrated in this study.

This study was limited by its cross-sectional design. A logical extension of this study would include longitudinal study of change in CCA in conjunction with measuring changes in other atrophy outcomes in relationship to disability. Future studies may also want to investigate the relationship between CCA and regional (deep and cortical) GMV. Addition of cognitive testing would further strengthen the significance of these results.

In conclusion, measurement of atrophy of the corpus callosum can have sensitivity as an imaging outcome in patients with MS, even in patients with low disability levels. Reliable

determination of corpus callosum atrophy is of importance because of the structure's known relationship with disability and cognitive dysfunction.

The first and corresponding authors take full responsibility for the data, the analyses and interpretation, and the conduct of the research. The first and corresponding authors guarantee the accuracy of the references. The funding source had no role in the study design or in the collection, analysis and interpretation of data. The Methods section includes a statement that IRB approval has been obtained for the use of human subjects for this study.

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